1 2 3 4 5 6 7 8 9	NOTICE: this is the author's version of a work that was accepted for publication in Nuclear Inst. and Methods in Physics Research, A. Changes resulting from the publishing process, such as peer review, editing, corrections, structural formatting, and other quality control mechanisms may not be reflected in this document. Changes may have been made to this work since it was submitted for publication. A definitive version was subsequently published in: Nuclear Instruments and Methods in Physics Research A 608 (2009) 410-416 doi:10.1016/j.nima.2009.07.022
10	A Digital X-ray Imaging System based on Silicon Strip Detectors
11	working in Edge-on Configuration
12	forming in Euge on Comiguration
13	L. Bolanos <sup>a</sup> , M. Boscardin <sup>b</sup> , A.E. Cabal <sup>a</sup> , M. Diaz <sup>c</sup> , P. Grybos <sup>d</sup> , P. Maj <sup>d</sup> ,
14	F. Prino <sup>e</sup> , L. Ramello <sup>f*</sup> , R. Szczygiel <sup>d</sup>
15	· · · · · · · · · · · · · · · · · · ·
16	<sup>a</sup> CEADEN, Calle 30 #502 e/ 5ta y 7ma Avenida, Playa, Ciudad Habana, Cuba;
17	<sup>b</sup> IRST, Fondazione Bruno Kessler, Via Sommarive 18, Povo, 38100 Trento, Italy;
18	<sup>c</sup> InSTEC, Ave. Salvador Allende esq. Luaces, Quinta de los Molinos, Ciudad Habana, Cuba;
19	<sup>d</sup> Faculty of Electrical Engineering, Automatics, Computer Science and Electronics, Department of
20	Measurement and Instrumentation, AGH University of Science and Technology, Al. Mickiewicza 30,
21	30-059 Cracow, Poland;
22	<sup>e</sup> Istituto Nazionale di Fisica Nucleare, Sezione di Torino, Via P. Giuria 1, 10125 Torino, Italy;
23	<sup>f</sup> Dipartimento di Scienze e Tecnologie Avanzate, Università del Piemonte Orientale, Via T. Michel 11,
24	15100 Alessandria, Italy.
25	*Correspondig author, e-mail: luciano.ramello@mfn.unipmn.it
26 27	Abstract – We present the energy resolution and imaging performance of a digital X-ray imaging
27	system based on a 512-strip silicon strip detector (SSD) working in the edge-on configuration. The
28 29	SSDs tested in the system are 300 $\mu$ m thick with 1 or 2 cm long strips and 100 $\mu$ m pitch. To ensure a
29 30	very small dead area of the SSD working in edge-on configuration, the detector is cut perpendicular to
31	the strips in a distance of only 20 $\mu$ m from the end of the strips. The 512-strip silicon detector is read
32	out by eight 64-channel integrated circuits called DEDIX (Grybos et al., 2007). The DEDIX IC
33	operates in a single photon counting mode with two independent amplitude discriminators per channel.
34	The readout electronic channel connected to a detector with effective input capacitance of about 2 pF
35	has an average equivalent noise charge (ENC) of about 163 el. rms and is able to count 1 Mcps of
36	average rate of input pulses. The system consisting of 512-channels has an excellent channel to channel
37	uniformity - the effective threshold spread calculated to the charge sensitive amplifier inputs is 12 el.
38	rms (at one sigma level). With this system a few test images of a phantom have been taken in the 10-30
39	keV energy range.
40	
41	Keywords – Silicon; strip; imaging; X-ray; amplifier.
42	

# 43 **1. Introduction**

44 45 Digital imaging systems based on silicon strip/pixel detector are widely used in high energy physics 46 experiments and X-ray imaging system [1]-[6]. However in case of X-ray imaging a standard 300 um thick detector converts nearly all 8 keV X-ray, but only ~26.7% of 20 keV X-ray and ~2% of 60 keV 47 48 X-ray. Therefore many laboratories are conducting intensive research on other semiconductor materials 49 with higher atomic number (like CZT, GaAs etc) [7]-[8]. There are also groups who make an effort to 50 build an effective imaging system for higher energy X-rays based on a silicon strip detector (SSD) in 51 edge-on configuration with the mechanical scanning [9]-[15]. The quality of such an imaging system is determined by several parameters and among them the most important are: (i) the small dead area of a 52 53 detector working in edge-on configuration and (ii) a low-noise multichannel readout electronics with 54 high count rate performance and short dead time.

In the present paper we present experimental results of 512-channel system built around the DEDIX
 64-channel ASIC [1]; preliminary results have been reported in [13].

57 We have already explored potential applications of this detector concept to dual energy medical 58 imaging, namely dual energy mammography [15] and K-edge angiography [16], and also to the K-edge 59 mapping of pigments in art paintings [17].

60 The paper is organized as follows. Section 2 describes the parameters of silicon strip used for operation

61 in edge-on configuration. Section 3 is a short description of the DEDIX integrated circuit architecture

1 and the 512-channel modules. The measurement parameters obtained with these modules are presented 2 in Section 4. Section 5 contains some examples of different images taken with this module and Section 3 6 summarizes the obtained results.

- 5 6

4

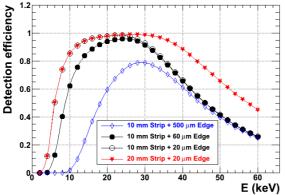
## 2. Silicon microstrip detector in edge-on configuration

7 Silicon microstrip detectors have reached technical maturity since many years, being widely used in 8 high energy physics mainly for charged particle (MIP) tracking. In the case of imaging with X-rays of 9 relatively low energy (10-60 keV) the main concerns are: efficiency, signal-to-noise ratio and rate 10 capability. The last two points depend mainly on the performance of the front-end electronics (see next Section), though of course the strip leakage current and the strip capacitance impact on the noise level. 11 12 The efficiency on the other hand depends on the detector geometry: the edge-on orientation helps to 13 keep a high efficiency. However in conventional detector designs the dead layer between the strips and 14 the physical edge (typically 500 µm) severely limits the efficiency at low energies.

In order to overcome this limit, we decided to implement the Current Terminating Structure (CTS) 15 16 [18] developed for the Roman Pots of the TOTEM experiment at LHC, which allows one to obtain 17 much reduced edge thickness. Figure 1 shows the computed efficiency for converting X-rays of 18 energies up to 60 keV in edge-on geometry, for 1 cm and 2 cm strip length and for edge thicknesses of 19 20 µm and 60 µm. For comparison also the case of 1 cm strips and 500 µm edge is shown. The 20 advantage of reduced edge thicknesses is evident in the 5-30 keV range, while the 2 cm length option is interesting particularly if the application requires energies around 50 keV (one such application is 21 22 imaging at the Gd K-edge).

23 The basic parameters of our detectors are: p+ strip on n-type substrate of 300 µm thickness, strip 24 pitch 100 µm. The detector is an AC coupled one with a punch-through bias structure. The detector 25 leakage current measured for a few selected detectors is below 500 pA/strip after cutting at 20 µm (this 26 is an average value which could be dominated by a few hot strips). The total strip capacitance is about 27 2 pF and 4 pF for the 1 cm and 2 cm strips, respectively. All detectors were designed and fabricated by 28 FBK-IRST, Trento, Italy.

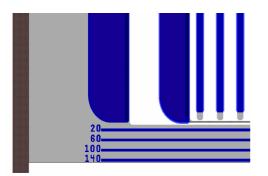
29



30 31 Fig. 1. Efficiency of conversion vs. X-ray energy for edge-on silicon detectors, with four choices of geometrical parameters. 32

33 A detail of the silicon strip detector layout is shown in Fig. 2, with a few strips, the guard ring and the 34 Current Terminating Structure visible. Each wafer contained four large 512-strip detectors, three with 1 35 cm long strips and one with 2 cm long strips, as well as other conventional strip detectors and test structures. The large detectors were characterized by their I-V curves, both for bias line (I<sub>BL</sub>) and guard 36 37 ring (IGR) currents, which were measured up to 100 V bias voltage, before and after wafer cutting at 38 either 60 µm or 20 µm from the physical edge.

39



1 2 3

4

11

15

Fig. 2. Layout of a corner of the SSD designed for edge-on utilization, shown before cutting. X-rays will be incident from the bottom. In the upper part, from right to left: three strips, guard ring, Current Terminating Structure. Cut lines at four different distances from the sensitive region are visible in the lower part.

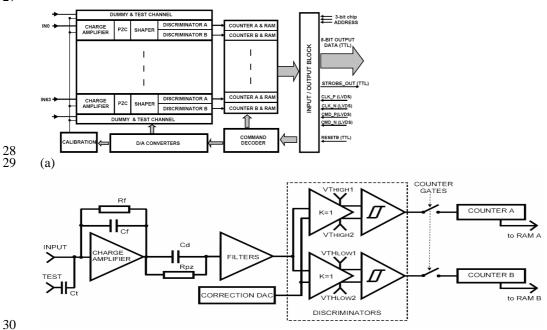
5 The current  $I_{GR}$  at 100 V was 1-2 mA after wafer cutting for all large detectors; the bias line current 6  $I_{BL}$  (sum over 512 strips) at 100 V showed instead huge variations, increasing of a factor between 2 and 7 9000 with respect to the uncut wafer value. We selected for further work three of the detectors showing 8 the lowest values of  $I_{BL}$  after cut, which are quoted as module I (1 cm strips, 60 µm cut), module II (2 9 cm strips, 20 µm cut) and module III (1 cm strips, 20 µm cut) in the next sections. Their  $I_{BL}$  at 100 V 10 after cut was in the range 100-200 nA.

12 3. Electronic read-out system13

# 14 3.1 Architecture of the DEDIX integrated circuit

16 The DEDIX integrated circuit comprises six basic blocks (see Fig. 3(a)): 64 analog front-end channels, 17 2×64 counters, an input-output block, a control command decoder, control DACs and a calibration 18 circuit. This integrated circuit (IC) is designed in the 0.35 µm Austriamicrosystems AG CMOS process 19 and the layout total area is 3900×5000 µm<sup>2</sup>. The block diagram of a single channel is shown in Fig. 20 3(b). Each channel is built of a charge sensitive amplifier (CSA) with a pole-zero cancellation (PZC) 21 circuit, a  $CR-RC^2$  shaper with a peaking time of 160 ns, two discriminators and two independent 20-bit 22 counters. The threshold voltages for two discriminators (A and B) in a single channel are set 23 independently, but are common for all 64 channels of the IC. Because from the CSA input up to the 24 discriminator inputs the signal processing chain is DC-coupled, a correction DAC (working in each 25 channel independently) is necessary to minimize the effects of the DC level spread at the discriminator 26 inputs. A detailed description of the DEDIX IC can be found in [1].





30 31 32

Fig. 3. The DEDIX Integrated Circuit: (a) block diagram, (b) scheme of a single channel.

(b)

# 3.2 Front-end modules

4 Three different 512-channel modules were built using silicon strip detectors in edge-on 5 configuration: modules I, II and III as quoted in the previous section. Each module contains 8 DEDIX 6 ICs which:

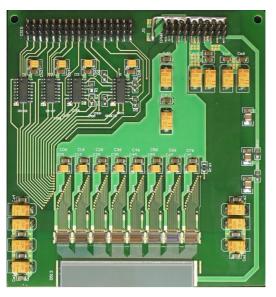
- in the case of modules I and II are connected to SSD having 1 or 2 cm long strips using a pitch
 adapter printed on a glass substrate – see Fig. 4(a),

9 – in the case of module III are connected directly to SSD having 1 cm long strips - see Fig. 4(b).

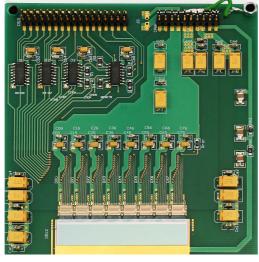
10

1 2

3



(a)



(b)

Fig. 4. Photographs of multichip modules with 512-silicon strip detector: (a) module I with 1 cm long detector with a glass pitch adapter, (b) module III with 1 cm long detector connected directly to ICs.

Module I is our first prototype, however because the pitch adapter adds some additional parasitic capacitance, a new printed circuit board (PCB) for module III was designed, which allows the direct bonding between the detector and the integrated circuits. The 6-layer PCB contains additional decoupling capacitors and low-voltage differential drivers (DS90LV031A) and receivers (DS90LV032A). Modules are controlled using a digital I/O card (National Instruments PCI 6534) plugged into a PC and all signals (clock, control and data) are transferred to or from the module using

17 LVDS standard. Data are collected with a program written in LabVIEW 8.2 (National Instruments).

In this configuration a single module is a row of 512 pixels with dimensions 100  $\mu$ m × 300  $\mu$ m. To obtain a 2D image, a mechanical scan in the direction perpendicular to PCB plane is used.

## 4. Measurement of the main parameters of 512-channel modules

## 4.1 Effective threshold spread and noise

1 2

3 4

5 6

7

8 In the case of DEDIX IC two discriminators thresholds A and B are common for all channels. The 9 critical aspect of such a solution is the channel to channel spread of the effective threshold levels. To 10 compensate this variation a 7-bit correction DACs (implemented in each channel of the IC) is loaded at 11 the system start-up. After loading the proper values of correction DACs, the spread of effective 12 threshold voltage in discriminators A in our module, as measured with fluorescence X-rays, is equal to 13 1.33 mV rms for all the 512 channels. If 3 channels with higher offset (namely no. 123, 289 and 290 -14 see Fig. 5(a) are excluded, the spread is reduced to 0.63 mV which, when referred to the input, 15 corresponds to about 12 el. rms (at one sigma level).

The measured spread for the discriminators B (set 240 mV below threshold A) is of about 6 mV and there are two reasons for this higher value of the spread: (i) the correction DAC in each channel is common for discriminators A and B, which have different input offsets, and values of correction DACs are optimised for discriminators A; (ii) the variation of the gain from die to die - see Fig. 5(b).

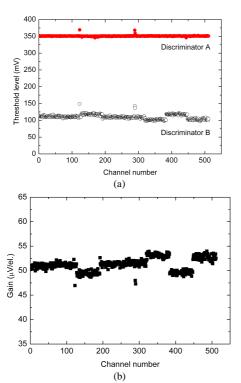


Fig. 5. (a) Spread of the effective threshold level for discriminators A set to average values of 350 mV and for discriminators B set at the same time to the average values of 110 mV. (b) Spread of the gain for module I.

21 For module I (with standard IC settings, power consumption 5 mW/channel) the mean gain is 51.2

 $\begin{array}{ll} 22 & \mu V/el. \mbox{ with standard deviation of } 1.33 \ \mu V/el \mbox{ - see Fig. 5(b)}. \mbox{ Setting the discriminators B for different} \\ 23 & energy levels than discriminators A causes that the effective threshold spread for discriminators B in \\ \end{array}$ 

24 our system is mainly determined by the die-to-die variations of the gain.

The spread of the effective discriminators levels is similar in all three modules. The measured equivalent noise charges for the tested 512-channel systems are summarized in Table I. The average ENCs for modules I, II and III are respectively:

- 193 el. rms (1 cm SSD with pich adapter),

- 29 243 el. rms (2 cm SSD with picth adapter),
- 30 163 el rms (1 cm SSD without pitch adapter).

31 Module II was operated at the same gain as module I, while in the case of module III we used a

different setting for lower current consumption (3 mW/channel), which resulted in an average gain of

 $33 \quad 38 \ \mu V/el.$ 

### TABLE I

Chip	Module I	Module II	Module III
Number	ENC [el. rms]	ENC [el. rms]	ENC [el. rms]
1	185	(*)	160
2	190	239	164
3	188	242	165
4	208	245	163
5	206	244	165
6	199	245	160
7	179	245	161
8	188	255	166

NOISE PERFORMANCE OF 8 ASICS INSTALLED ON PCB

6 (\*) Chip was mechanically damaged during the measurements.

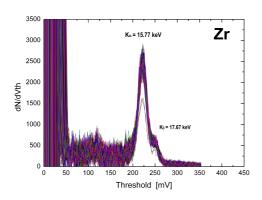
# 8 4.2 Energy resolution

The energy resolution of our system is determined by the noise performance of the readout electronics which is enough good for the foreseen applications. The small threshold spread in the system allows the effective photon counting in a given energy window. Two examples of measured energy spectra of Zr and Sn are shown in Fig. 6(a) and 6(b).



7

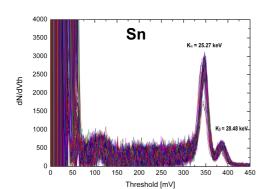
9



15 16

17 18

19



Two channels with lower number of counts are situated on edge of the detector.

20

Fig. 6(b). Energy spectra measured in 509 channels of module I (edge-on configuration) using threshold scan for Sn fluorescence. Two channels with lower number of counts are situated on edge of the detector.

Fig. 6(a). Energy spectra measured in 509 channels of module I (edge-on configuration) using threshold scan for Zr fluorescence.

In the case of Sn spectra (see Fig. 6(b)) one can easily distinguish  $K_{\alpha}$  and  $K_{\beta}$  peaks separated only by 3.2 keV.

25 For a system using mechanical scan to obtain 2D-imaging the important parameters are high count rate

- 26 performance and short data readout time (dead time of the system). As it is shown in [1] the analog
- 27 parameters of DEDIX IC do not degrade up to 1 Mcps of average rate of input pulses. Another
- 28 important issue is the dead-time of the IC. After the exposure time the counter gates are switched off

(see Fig. 3.b), the values of 20-bit counters are loaded into RAMs and the counters are reset. With 30
 MHz clock these operations last about 340 ns. This buffering scheme ensures that the data readout and
 counting of the input pulses can be performed simultaneously and no additional noise counts are
 registered in this mode. In the readout mode separate from exposure the readout time of single IC is

5 16.7  $\mu$ s, and for the 8 chip module is of about 133  $\mu$ s (with 30 MHz clock).

# 5. Imaging test

6 7

8

9 We acquired test images of the phantom sketched in Fig. 7 exploiting a mechanical scan with 300 µm step. The goal was to validate the concept of obtaining 2D images with our 1D strip detector using a monochromatic X-ray beam, rather than optimizing the signal-to-noise ratio.

The setup consisted of a 2 kW Cu-anode X-ray tube (maximum voltage 60 kV, maximum current 60 mA for voltages up to 30 kV, 50 mA for 40 kV), a set of interchangeable fluorescence targets (oriented at 45° with respect to the primary beam, dimensions 25 by 25 mm<sup>2</sup>), a secondary beam at 90° with respect to the primary beam, a phantom and a silicon strip detector.

The phantom consisted of a plexiglass slab 5.6 mm thick, with various hollows and inserts (see Fig.
7); it was mounted on a moving holder placed at 60 cm from the fluorescence target, perpendicular to
the secondary beam.

The silicon strip detector (module III) was in a fixed position at 70 cm from the target, with edge-on orientation (strips parallel to the secondary beam); a sensitive region 300 µm wide (detector thickness) and 51.2 mm high (512 strips) was then available. Due to the distance between the target and the detector, the secondary beam flux was rather uniform along the 512 strips. A flat-field correction was applied to the raw images.

The images were obtained by moving the phantom across the detector with a step equal to the detector thickness; a pixel of the following images is therefore 300 µm by 100 µm. The typical acquisition time was 40 s per scanning step, i.e. a total time of 80 minutes for 120 steps, limited by the low luminosity of fluorescence X-rays in our set-up: 2500 counts/mm<sup>2</sup>/s or about 75 counts/pixel/s. Images were processed using the ROOT framework [19].

29

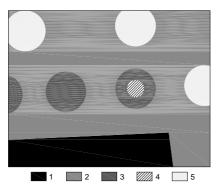


Fig. 7. Front view of the phantom (only the imaged area, about 51 mm  $\times$  36 mm). Region 2 (the body) is a plexiglass slab 5.6 mm thick. Cylindrical hollows 2.95 mm deep machined in the plexiglass contain either wax (region 3) or air (region 5). Inside the wax there is a thin aluminium foil (region 4) of thickness 75  $\mu$ m. Region 1 is a brass foil used for alignment purposes.

Figure 8(a) shows the final image obtained with the highest fluorescence energy available in our setup, namely that of Sn, with  $K_{\alpha}$  peak at 25.3 keV and  $K_{\beta}$  peak at 28.5 keV. Thresholds A and B were set such that we could use discriminators B counts to subtract the Sn- $K_{\beta}$  contribution from the final image, which is therefore an image at 25.3 keV. It is evident that the contrast is not very good and the Al insert within the wax is barely visible. Numerical values of contrast between different regions i and j (defined in Fig. 7) are reported in Table II; the contrast is defined as  $(C_i-C_j)/C_2$  where  $C_i$  and  $C_j$  are the averages of counts in region i and j (so the contrast is always normalized to the counts in region 2), and its error is defined as  $\sqrt{(rms_i^2-rms_i^2)/C_2}$ .

Figure 8(b) shows the final image obtained with a lower fluorescence energy, namely that of Zr, with K<sub> $\alpha$ </sub> peak at 15.8 keV and K<sub> $\beta$ </sub> peak at 17.7 keV. Since this K<sub> $\beta$ </sub> peak cannot be resolved by our system (see Fig. 6(a)), we set the threshold of discriminators B just above the Zr K<sub> $\beta$ </sub> peak, in order to subtract the counts due to continuum photons at higher energies. In the case of Fig. 8(b) the contrast is much better than Fig. 8(a), and the Al insert is clearly visible. Numerical values of contrast between different regions are again reported in Table II. 1 Finally, Fig. 8(c) shows the final image obtained with the lowest fluorescence energy, namely that of 2 Ge. Since the  $K_{\beta}$  peak of Ge cannot be resolved by our system, we set the threshold of discriminators B 3 just above the  $K_{\beta}$  peak, in order to subtract the counts due to continuum photons at higher energies. In 4 the case of Fig. 8(c) the contrast (Table II) is even better than Fig. 8(b), and the Al insert is clearly 5

- visible.
- 6 Signal-to-noise ratios (SNR) are presented for the three images in Table III. SNR is defined as (Ci-
- 7 C<sub>i</sub>)/rms<sub>2</sub> where C<sub>i</sub> and C<sub>i</sub> are the counts (corrected for flat-field) in ROIs of size 10×10 pixels defined in
- 8 regions i and j (defined in Fig. 7) and rms<sub>2</sub> is the rms fluctuation of the counts in region 2, defined with
- 9 a  $1 \times 1$  pixels noise sampling area. The air-plexiglass SNR is in each case acceptable (i.e. greater than 5
- 10 as dictated by the Rose criterion), while the Al-wax SNR is barely acceptable only for the case of Ge
- 11 target. It must be noted that the latter image suffers from lower statistics with respect to other images
- 12 (counts in the plexiglass region for Ge target are only about 1/4 with respect to Sn and Zr ones) and this
- 13 is especially visible in the SNR values between regions 2 and 3.

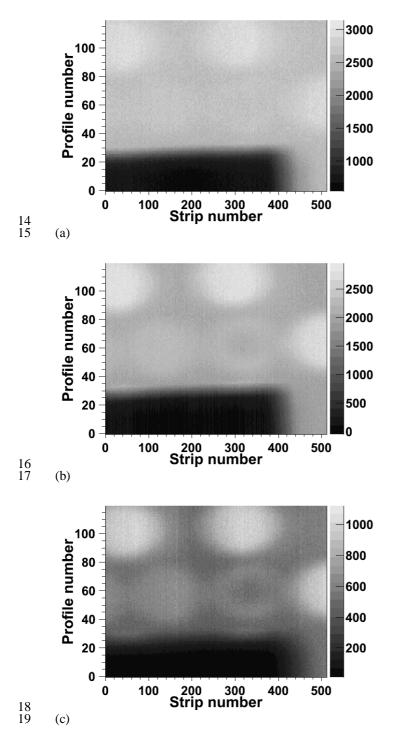


Fig. 8. Images of the phantom (horizontal axis: 512 strips at 100 µm pitch; vertical axis: 120 scanning steps at 300 µm pitch) collected with fluorescence X-rays from: (a) Sn target  $-K_a$  peak at 25.3 keV,  $K_b$  peak at 28.5 keV; (b) Zr target  $-K_a$  peak at 15.8 keV,  $K_{\beta}$  peak at 17.7 keV; (c) Ge target -  $K_{\alpha}$  peak at 9.9 keV,  $K_{\beta}$  peak at 11.0 keV. The scales of grays on the right-hand side of each image represent the counts, corrected for flat-field.

#### TABLE II

CONTRAST BETWEEN DIFFERENT PARTS OF THE IMAGES

Regions involved	Sn image contrast	Zr image contrast	Ge image contrast
2-5	$0.118 \pm 0.030$	$0.329 \pm 0.037$	$0.692 \pm 0.074$
2-3	$0.024 \pm 0.028$	$0.111 \pm 0.038$	$0.115 \pm 0.077$
3-4	$0.024 \pm 0.027$	$0.104 \pm 0.037$	$0.238 \pm 0.067$

#### TABLE III

SIGNAL-TO-NOISE RATIO IN DIFFERENT PARTS OF THE IMAGES

Regions involved	Sn image SNR	Zr image SNR	Ge image SNR
2-5	5.95	11.6	13.6
2-3	1.20	3.90	2.26
3-4	1.21	3.65	4.68

10

11 12

13 14

15

16

17

18 We have not fully exploited the high rate capability of our system, namely 1 Mcps per channel (see 19 previous section); for this purpose, dedicated 2D imaging tests with higher flux of X-rays at a 20 synchrotron facility [10] or with a dual energy setup [20,21] would be appropriate. A factor 1000 21 increase of the counts/pixel/s can be anticipated, reducing the acquisition time quoted earlier from 80

22 minutes to 5 seconds.

23 The obtained system performance and the imaging test suggest that our 512-strip modules can find 24 useful applications, among others, in digital radiography – both dual energy mammography [15] and 25 angiography with the K-edge subtraction technique [18] - and in the mapping of pigments of art 26 paintings [17]. The K-edge subtraction technique requires two such modules placed a few mm apart, 27 respectively dedicated to energies below and above the K-edge; energies of interest range from about 28 10 keV up to 50 keV (Gd K-edge). In the case of dual energy mammography, the two energy 29 components of the beam will be detected by a single module, thanks to the availability of 30 discriminators A and B.

31

#### 32 6. Summary 33

34 We have presented a 512-channel module based on Silicon Strip Detectors working in edge-on

35 configuration with a very small dead area of the detector. The comparison of our system with other

36 systems working with silicon strip detector in edge-on configuration is presented in Table IV.

37 The noise, channel-channel uniformity and count rate performance make the system promising for 2-D

38 imaging in the range of low and medium energy range of X-rays. Images of a phantom taken with

39 fluorescence X-rays at different energies demonstrate the imaging capabilities of the system in edge-on

40 configuration even at low X-ray energies.

<sup>1</sup> 2345 6789

TABLE IV

COMPARISON OF SYSTEMS WORKING WITH SILICON STRIP DETECTOR IN EDGE-ON CONFIGURATION

Reference	[11,22]	[9, 23]	[12]	[14,15]	This work
Strip pitch × detector thickness [μm × μm]	$100 \times 300$	$500 \times 500$	100 × 300	$100 \times 300$	$100 \times 300$
Dead layer of detector [µm]	-	-	240	765	20
Number of channels	16	1000	384	384	512
Noise [el. rms]	40	190 <sup>a</sup>	500	200	163
Shaper peaking time [ns]	50 <sup>b</sup>	500	75	800	160
Max count rate per channel [MHz]	2	-	3.5	0.1	1
Threshold spread - std dev [el.]	300	24.5	-	87	12
Energy window	no	yes	no	yes	yes

<sup>(a)</sup> noise without detector

<sup>(b)</sup> minimum peaking time

## Acknowledgements

The authors are grateful to M. Gambaccini from University of Ferrara for providing the phantom. 11 The authors from the AGH University of Science and Technology gratefully acknowledge the 12 13 opportunity to be a member of the Cadence Academic Network, providing us with a very valuable 14 knowledge and methodology exchange plat-form. We gratefully acknowledge Floreana Dumitrache 15 and Barbara Pini from INFN Torino and Maciej Kachel from AGH UST Cracow for their careful 16 bonding work.

17 This work was supported by Ministry of Science and Higher Education, Poland and Istituto 18 Nazionale di Fisica Nucleare, Italy.

#### References

19 20

- [1] P. Grybos, et al.: "Measurements of Matching and High Count Rate Performance of Multichannel ASIC for Digital X-Ray Imaging." IEEE Trans. Nucl. Sci,. vol. 54, 2007, pp. 1207-1215.
- [2] X. Llopart, M. Campbell, R. Dinapoli, D. San Segundo, E. Pernigotti, "Medipix2: a 64-k Pixel Readout Chip With 55-µm Square Elements Working in Single Photon Counting Mode.", *IEEE Trans. Nucl. Sci.*, vol. 49, no. 5, 2002, pp. 2279 - 2283. [3] Ch. Bronnimann, et al.: "A pixel read-out chip for PILATUS project." *Nucl. Instrum. Methods A*, vol. 465, 2001, pp. 235-
- 239.
- [4] R. Rossi, P. Fischer, T. Rohe, N. Wermes "Pixel Detectors. From Fundamentals to Applications", Springer-Verlag, Berlin, Heidelberg 2006.
- [5] Y. Allkofer et al., "Design and performance of the silicon sensors for the CMS barrel pixel detector" Nucl. Instrum. Methods, vol. A584, 2008, pp. 25-41.
- [6] H.J. Simonis, "Status of the silicon strip detector at CMS" Nucl. Instrum. Methods, vol. A598, 2009, pp. 46-49.
- [7] G. De Geronimo, P. O'Connor, J, Grosholz "A generation of CMOS readout ASICs for CZT detector." IEEE Trans. Nucl. Sci., vol.47, no.6, pp. 1857-1876, Dec. 2000.
- [8] L. Tlustos et al., "Characterisation of an epitaxial GaAs/Medipix2 detector using fluorescence photons" Nucl. Instrum. Methods, vol. A591, 2008, pp. 42-45.
- [9] B. Hilt, P. Fessler, G. Prevot, "New quantum detection system for very low dose X-ray radiology." Nucl. Instrum. Methods, vol. A442, 2000, pp. 38–44.
- [10] C. Venanzi, A. Bergamaschi, D. Derossi, S. Olivo, S. Pani, R. Longo, et al., "A digital detection system for synchrotron radiation breast tomography" IEEE NSS-MIC 2004 Conference Record.
- [11] E. Beuville, R. Cahn, B. Cederstrom, M. Danielsson, A. Hall, B. Hasegawa, et al., "High resolution X-ray imaging using a silicon strip detector." IEEE Trans. Nucl. Sci., vol.45, no.6, pp. 3059-63, Dec. 1998.
- [12] E. Verbitskaya, et al., "Advanced Model of Silicon Edgeless Detector Operation" IEEE NSS-MIC 2008 Conference Record, pp. 2711-2716.
- [13] L. Ramello, et al.: "Development of a 512-channel Module for Digital X-ray Imaging Systems with SSD" Poster P3-17 presented at the Xth EFOMP Congress - First European Conference on Medical Physics, Castelvecchio Pascoli, Italy, 20-22 September 2007
- [14] P. Grybos, et al.: "RX64DTH A fully integrated 64-channel ASIC for a digital X-ray imaging system with energy window selection." IEEE Trans. Nucl. Sci., vol. 52, 2005, pp. 839-846.
- [15] C. Avila et al., "Contrast cancellation technique applied to digital x-ray imaging using silicon strip detectors", Med. Phys. 32 (2005) 3755-3766.
- [16] A. Sarnelli et al., "K-edge digital subtraction imaging based on a dichromatic and compact x-ray source" Phys. Med. Biol. 49 (2004) 3291-3305.
- [17] P. Baldelli et al.: "Application of the K-edge X-ray technique to map pigments of art paintings: Preliminary results" Nuovo Cim., vol. 29C, 2006, pp. 663-672.
- [18] G. Ruggiero et al.: "Planar edgeless silicon detectors for the TOTEM experiment" IEEE Trans. Nucl. Sci., vol. 52, 2005, pp. 1899-1902.

6

7

- 123456789[19] R. Brun and F. Rademakers, "ROOT - An Object Oriented Data Analysis Framework" Nucl. Instrum. Methods, vol. A389,
- 1997, pp. 81–86; see also http://root.cern.ch [20] M. Gambaccini et al.: "Narrow energy band x-rays via mosaic crystal for mammography application" *Nucl. Instrum.* Methods, vol. A365, 1995, pp. 248-254.
- [21] A. Tuffanelli et al.: "Evaluation of a dichromatic x-ray source for dual-energy imaging in mammography" Nucl. Instrum.
- Methods, vol. A489, 2002, pp. 509–518. [22] E. Beuville et al.: "An application specific integrated circuit and data acquisition system for digital X-ray imaging" *Nucl.* Instrum. Methods, vol. A406, 1998, pp. 337-342.
- [23] P. Fessler et al.: "An important step forward in continuous spectroscopic imaging of ionising radiations using ASICs" Nucl.
- 10 Instrum. Methods, vol. A421, 1999, pp. 130-141.